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Impact of endodontic irrigants on surface roughness of various nickel-titanium rotary endodontic instruments



Tamer M. Hamdy^{1*}, Yasmine Mohsen Alkabani¹, Amira Galal Ismail¹ and Manar M. Galal¹

Abstract

Background The aim of the current study is to assess the surface roughness of several recent nickel-titanium (Ni-Ti) rotary endodontic instruments, namely: Protaper next (PTN); Hyflex CM (CM); Hyflex EDM (EDM); WaveOne gold (WOG); and trunatomy (TN), before and after application of 5.25% sodium hypochlorite (NaOCI) irrigant solution.

Methods In this in vitro study, five recently introduced rotary endodontic instruments of different metallurgical properties and designs were subjected to Atomic Force Microscopy (AFM) analysis, and then each file was rotated in 5.25% NaOCI for 15 min., with speed and torque according to manufacturer's instructions. The instruments were then subjected to AFM analysis again. The surface roughness average (Sa) parameter was calculated. Data were analyzed by Paired T test, One-way ANOVA and Tukey tests.

Results There was a statistically significant decrease in the surface roughness of all rotary endodontic instruments after immersion in irrigants ($P \le 0.05$).

Conclusion The new TN and PTN instruments showed the least surface roughness. All tested Ni-Ti rotary endodontic instruments after irrigants exposure showed a varying increase in surface roughness.

Keywords Atomic Force Microscopy, Surface roughness, Irrigation, Sodium Hypochlorite, Ni-Ti, rotary instruments

Background

Several manufacturing approaches and modifications have been developed to enhance mechanical properties and reduce the incidence of rotary file fracture, which led to effective endodontic treatment outcomes [1-3]. The process of Ni-Ti alloy cold working induces stressed areas that are predisposed to the formation of cracks or brittle fractures [4, 5]. Therefore, continuous improvements in Ni-Ti endodontic instruments could be achieved

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endodontic instruments at normal mouth temperature, allowing maximum flexibility to be gained [6]. Moreover, heat treatment could also improve their resistance to cyclic fatigue compared to conventional Ni-Ti alloys. Ni-Ti endodontic instruments could be described as those mostly comprising the austenitic phase and those mostly containing the martensitic phase [7]. Endodontic instruments based on austenitic alloys possess superelastic properties. On the contrary, endodontic instruments based on martensitic alloys (M-wire) demonstrated a shape memory effect, became ductile, easily deformed, and exhibited more flexibility [6, 7].

through thermal, mechanical, and electrical treatment

to impart a more stable martensite phase into the Ni-Ti

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The Ni-Ti instrument's surface topography could be altered by manufacturing composition, heat treatment, geometrical designs, and mechanical stresses [2, 5]. For example, HyFlex CM (CM) rotary instrument (HCM; Coltene/Whaledent AG, Altstätten, Switzerland) is a controlled shape memory wire, has a stable martensitic microstructure at the mouth temperature which enhance their flexibility [8]. It is machined from a wire subjected to previously a thermo-mechanical process. The manufacturer has claimed that CM instrument has substantially enhanced flexibility and fatigue resistance which considerably decrease the incidence of instrument separation [9]. The Hyflex EDM (EDM) instruments (HEDM; Coltene/Whaledent AG, Altstätten, Switzerland) was processed using controlled electrical discharge machining method. The EDM process is a contact-free machining process used for manufacturing of parts that are difficult to machine with conventional grinding techniques [8, 10]. These techniques based on electrical sparks which provide a local melting to the materials with subsequent partial evaporation of minute parts of metals leaving superficial irregularities referred to "crater-like" surface finish. It is claimed that EDM instruments had high cyclic fatigue resistance [2, 8]. The ProTaper Next (PTN) instrument (PTN; Dentsply Maillefer, Ballaigues, Switzerland) is M-wire, thermally processed to enhance their flexibility and decrease the stresses concentration, its design include different tapers with a rectangular and off-centered cross-sectional area [11]. The Wave One Gold (WOG) instruments (WOG; Dentsply Maillefer, Ballaigues, Switzerland) used in reciprocating motion, is fabricated using M-wire using a heat-treatment process. It produces parallelogram-shaped cross-Sect. [12]. Recently introduced TruNatomy (TN) rotary instruments (TN; Dentsply Sirona, Baillagues, Switzerland) is subjected to heat treatment annealing, it provides a slender shape than improve the debridement process. Manufacture claim that TN instrument are extremely flexible and have a high cyclic fatigue resistance [13, 14]. Table 1

Table 1 Type of alloy and composition of Ni-Ti instruments

Ni-Ti system	Type of alloys	Composition
Hyflex CM	CM wire	Martensite with various amounts of austenite and R-phase
Hyflex EDM	CM wire using electrical discharge machining	No austenite phase
Protaper Next	M-Wire	Mainly austeNi-Tic phase with little amounts of R- phase and martensite
Wave One Gold	M-Wire using gold thermo-mechanical heat treatment	Mainly stable martensite or R-phase
TrueNatumy	Proprietary novel heat treatment technique	R-phase and martensitic transformation

summarized the types of alloys, composition and properties of some Ni-Ti instruments [2, 6, 15].

Endodontic irrigants are used for a variety of biological, chemical, and mechanical purposes which are critical for successful root canal treatment [16–19]. It is advised to constantly perform root canal instrumentation under copious irrigating solution [19].When the irrigant encounters Ni-Ti instruments, this may lead instrument corrosion, deformation, surface roughness enhancing mechanical failure [5, 20, 21]. Amongst currently used irrigating solutions, NaOCl in 5.25% appears to the most commonly used and effective root canal irrigants [16, 22, 23].

The contact between Ni-Ti instruments and irrigants may be induce an instrumental corrosion and flaws accelerating instrument's cyclic fatigue and failure [24]. There is a strong relation between fracture mechanism and surface characteristics of rotary Ni-Ti instruments [25, 26].Repeated irrigation is reflected by reduction in Ni-Ti rotary endodontic instruments cutting efficiency and increase in their surface roughness [27, 28]. The surface roughness investigation of Ni-Ti rotary instruments offers convenient evidence concerning surface defects and performance [5]. AFM is one of the most widely used imaging tools used to assess surface topography accurately. AFM allows a topographic mapping of the surface using a non-destructive probes [5, 29].

Recently, there have been limited studies considering the surface roughness of the recently introduced Ni-Ti rotary instrument for assessment of this value before and after exposure to root canal irrigation [26, 30, 31]. Hence, the aim of the study is to evaluate the impact of endodontic irrigants on the surface roughness of several Ni-Ti rotary endodontic instruments. The null hypothesis was that there was no significant difference regarding surface roughness between Protaper Next (PTN), Hyflex CM (CM), Hyflex EDM (EDM), WaveOne Gold (WOG), and Trigonometry (TN) rotary Ni-Ti instruments before and after application of 5.25% sodium hypochlorite (NaOCl) irrigant solution.

Methods

Sample size was calculated using G*Power (version 3.1.9.7) sample size calculator via means and standard deviations [32]. The estimated sample size required 10 endodontic rotary instruments in each group. The Medical Research Ethical Committee (MREC) of National Research Centre (NRC); Cairo, Egypt approved the research (Reference number: 24,312,012,023).

In the present study Protaper next (PTN; Dentsply Maillefer, Ballaigues, Switzerland), Hyflex CM; Coltene/Whaledent AG, Altstätten, Switzerland), Hyflex EDM; Coltene/Whaledent AG, Altstätten, Switzerland), WaveOne gold (WOG; Dentsply Maillefer, Ballaigues, Switzerland) and trunatomy (TN; Dentsply Maillefer, Ballaigues, Switzerland) were included. A new endodontic rotary instrument of each brand was examined and inspected under a scanning electron microscope (SEM) (Olympus soft imaging solutions, GMBH, Muenster, Germany) before performing the test, any distorted or faulty endodontic rotary instruments were excluded. The selected size of endodontic rotary instruments was 25 at the tip, with taper of 0.06 and a length of 25 mm. The irrigants employed were 5.25% NaOCl (Tianshi Biological Technology Co. Ltd, Henan, China).

Ten new endodontic rotary instruments of each brand were analyzed using AFM (Tosca 200 AFM, Anton Paar GmbH, Ostfildern, Germany). Analysis perormed using software Mountains 8 (Digital Surf, Besançon, France). AFM images were taken in tapping mode under ambient conditions at resolution 400, with rate 1 line/ second at angle 0 degree.

Analysis of each brand was performed before irrigation and then again after irrigation. Irrigation was done by immersion of each rotary instrument into 5.25% NaOCl for 15 min at 37 °C.

The dynamic immersion was done by rotating the endodontic rotary instruments attached to an endodontic motor (X-Smart Plus Endomotor, Dentsply Sirona, Ballaigues, Switzerland) and rotating freely at a constant speed (400 rpm) under constant torque (2.5 Ncm) into Eppendorf plastic tubes of 2 mL (Deltalab, S.L., Barcelona, Spain) containing 2 mL of 5.25% NaOCl irrigant solution for 15 min, which represent the clinical conditions during root canal therapy [33]. All the endodontic rotary instruments after removing from irrigant solution were rinsed with distilled water to neutralize the effect of irrigation and dried.

Each brand of endodontic rotary instrument was placed on the specimen stage of the AFM device, with the handle always in the same position. The same selected areas were examined before and after exposure to irrigants.

Table 2Mean and Standard Deviations of Sa parameter surfaceroughness before and after immersion of investigated rotaryendodontic instruments (nm)

Rotary endodontic instruments	c Surface roughness Sa values (nm)		P value
	Before	After	_
	immersion	immersion	
CM	58.5 ^b ±7	$74.9^{a} \pm 1.1$	P=0.04*
EDM	$67.9^{\circ} \pm 5$	81.1 ^b ±3.1	P=0.001*
PTN	$49.8^{a} \pm 7.1$	$68.0^{a} \pm 8$	P=0.0001*
WOG	$66.6^{b} \pm 8.6$	$84.1^{\circ} \pm 2.4$	P=0.0001*
TN	$38.8^{a} \pm 1.3$	83.1 ^{bc} ±1.8	P=0.0001*
P value	P=0.0001*	P≤0.04*	

Means in same row have no letters as they are only two groups (before and after irrigation), while means in same column with different letters indicate significance difference. *Corresponds to significant difference ($P \le 0.05$)

The endodontic rotary instruments were attached to a glass plate using a double-sided adhesive for evaluation of the cutting blade and the flute between the instruments. Each specimen was mounted on the AFM, and then 10 consecutive points positioned on a 4 mm section of the tip of each rotary instrument were examined; the scanned areas were $1 \times 1 \ \mu m^2$ squares [34, 35]. The AFM images were recorded in tapping mode under ambient conditions. AFM analysis software was employed to process a three-dimensional (3D) image, and surface roughness parameters were evaluated using the Sa parameter.

The null hypothesis was that there would be no significant difference in mean Sa values among PTN, CM, EDM, WOG, and TN Ni-Ti instruments before and after immersion in 5.25% NaOCl irrigants.

Statistical analysis

Data were analyzed using the Statistical Program for the Social Sciences (SPSS Inc., Chicago, IL, USA). Shapiro-Wilkes test was applied for the assessment of normality. Paired t-test was performed to detect the effect of the irrigant on the surface roughness of the endodontic instruments, by measuring the average surface roughness (Sa) before and after irrigation. While One-way ANOVA and Tukey tests were used to compare the surface roughness of the different instruments before irrigation. Similarly, the surface roughness of the different instruments was compared after irrigation. Significant difference was considered when $P \le 0.05$.

Results

The mean and standard deviations of the Sa values are displayed in Table 2; Figs. 1, 2, 3, 4 and 5. There was a significant increase in surface roughness (Sa) in all tested rotary endodontic instruments after immersion in the irrigants.

Comparing the surface roughness of the different instruments before irrigant application amongst all groups showed that TN and PTN showed the least roughness with a P value= 0.0001^* compared with other instruments with no significant difference between them (P=0.7) while they were significantly different from the other instruments (P= 0.0001^*). This is followed by WOG and CM with no significant difference between them (P=1) while they were significantly different than the other instruments (P= 0.0001^*). The EDM showed highest roughness compared to other instruments (P=0.04with CM and P= 0.0001^* with the rest of instruments).

Comparing the surface roughness of the different instruments after irrigants application amongst all groups showed that CM and PTN showed the least roughness with a P value of 0.0001^* compared with other instruments, with no significant difference between them (P=1), while they were significantly different from the







Fig. 2 AFM imaging of EDM instruments (a) before immersion in irrigants, (b) after immersion in irrigants



Fig. 3 AFM imaging of PTN instruments (a) before immersion in irrigants, (b) after immersion in irrigants



Fig. 4 AFM imaging of WOG instruments (a) before immersion in irrigants, (b) after immersion in irrigants



Fig. 5 AFM imaging of TN instruments (a) before immersion in irrigants, (b) after immersion in irrigants

other instruments ($P \le 0.01^*$). This is followed by EDM and TN with no significant difference between them (P=0.8), while they were significantly different from the other instruments ($P \le 0.04^*$). The WOG showed highest roughness compared to other instruments ($P \le 0.03^*$) except TN; as no significant difference was detected among WOG and TN (P=0.3).

Discussion

The current study is the first to evaluate the surface roughness of CM, EDM, PTN, WOG, and TN Ni-Ti instruments at the nanoscale before and after immersion in a 5.25% NaOCl irrigant solution using 3D AFM. Application of NaOCl at 5.25% is currently considered the gold standard for root canal irrigants [16, 23]. Surface features of Ni-Ti endodontic rotary instruments should be properly considered when evaluating their quality. Surface irregularities can potentially compromise corrosion resistance, and the cutting effectiveness of endodontic rotary instruments affects corrosion resistance [33, 36]. Ni-Ti endodontic rotary instruments corrosion starts with the selective removal of nickel from the alloy surface when

the instrument is subjected to sodium NaOCl during the root canal treatment [14].

The surface irregularities could be assessed by evaluating the surface roughness [35].The surface roughness characterization of Ni-Ti endodontic rotary instruments delivers beneficial data concerning surface defects and performance [37]. Therefore, studies have been carried out using various techniques, including SEM, AFM and non-contact optical profilometry to examine the surface topography of endodontic instruments [5]. The SEM modality provided two-dimensional (2D) images were difficult to be administer for quantitative surface data [38]. AFM creates 3D topographical images that provide information about surface morphology and defects [39]. The AFM was a valuable, practical, and non-destructive technique for quantitative assessment of the surface topography of the Ni-Ti rotary instruments [30, 35].

Surface roughness might be expressed by various parameters. The modalities Sa, Sq, Sz were mostly to be utilized for endodontic instrumental surface analysis [40, 41]. The surface roughness average (Sa) topographical parameter represents the arithmetical mean height of

the surface and expresses a class of amplitude parameters counting the properties of technical surfaces [42]. This parameter is generally used to evaluate surface roughness; it is used to investigate the vertical surface topography of endodontic rotary instruments and perform the comparison [32, 35]. It is well recognized that defects in surface microstructure may cause areas of stress concentration and the creation of cracks, which sequentially weaken the structural integrity of the Ni-Ti instrument [43–45].

The results revealed that the unused new brands of Ni-Ti instruments showed various degrees of Sa before irrigation. This observation may be due to the presence of surface defects and irregularities created during the process of manufacturing Ni-Ti instruments, which produce nano-scale surface irregularities, even in unused instruments [32, 35, 36, 46].

TN and PTN demonstrated the lowest Sa values. The lower Sa values of TN instruments may be attributed to their surface, which minimizes the residual machining defects from the fabrication procedure [47]. In addition, the thermo-mechanical processing gained by the special heat treatment of Ni-Ti wire could overcome the machining procedure faults through modification of their crystalline phase [2, 48]. Moreover, the lower Sa values of PTN instruments may be due to their fabrication from M-wire, which is thermally treated during manufacturing to improve flexibility and increase fatigue resistance [5, 49].

WOG and CM demonstrated higher Sa values than other instruments. These findings may be due to the fact that WOG manufacturing undergoes heat treatment of the alloy (gold wire) to machine a parallelogram-shaped cross-section, which may affect the surface characteristics of NiTi, leading to a rougher or even porous surface [5]. Similarly, the cause of the rougher surfaces of CM instruments may be attributed to their production procedure in a special thermo-mechanical process that aims to increase the flexibility of traditional NiTi files [50]. However, the highest Sa values of EDM may be due to the electrical discharge machining technology, which is based on the vaporizing and melting of the small particles on the surface by the action of electric sparks and shaping, which induces surface irregularities [50, 51].

Concerning Sa after irrigation, amongst all tested Ni-Ti instruments, all the tested Ni-Ti rotary endodontic instruments exhibited varying amounts of Sa values after exposure to irrigants. These findings may be due to the deterioration effect of NaOCl on the Ni-Ti instrument surface. The exposure of the metal to NaOCl irrigants may lead to corrosion and the subsequent production of cracks and pits that affect the surface integrity of the Ni-Ti instrument [1, 44, 52]. The results showed that CM and PTN demonstrated the lowest Sa values; this finding may be due to the fact that the CM instrument had a uniform surface topography [51]. These findings may also be due to the martensite grains of M-wire and their smaller grain size than other Ni-Ti wires, which are responsible for increasing their wear resistance and strength. Also, they concluded that the smaller grain sizes of the alloy can inhibit crack initiation through the grain boundaries [28, 53, 54].

Moreover, PTN instruments, which were produced from an M-wire and subjected to pre-machining heat treatment, may be the cause of reducing the surface cracks upon instrumentation [55]. Furthermore, the results showed that EDM and TN demonstrated a higher Sa value. The electrical sparks used during the fabrication process of EDM instruments may be responsible for the creation of surface roughness that could improve the cutting efficiency of tools but produce micropores, which are referred to as corrosion pits, which are associated with crack initiation and encourage corrosion by the action of NaOCl [15, 51, 53, 56].

While TN exhibited more surface roughness, which may be explained by the fact that proprietary postmachining heat treatment manufacturing processes may induce inherent characteristics that reduce their resistance to corrosion on exposure to irrigants [15, 57]. Our results showed that WOG demonstrated the highest SA value. This may be attributed to the fact that WOG undergoes thermal treatment before and after instrument machining [58]. Additionally, heat treatment employed during manufacturing may alter the Ni-Ti surface characteristics, resulting in a rough or porous surface [5, 31, 59].

In summary, it was noted that manufacturers use various methods of surface treatment, such as ion implantation, thermal nitridation, cryogenic treatment, nitride coating, and electropolishing, to tackle processing defects [57, 60]. But these processes may counteract the irrigation steps, interact with the chlorine ions in the irrigation solutions, and affect the surface integrity.

The present study has evaluated the endodontic rotary instruments in an in vitro situation, which is considered a limitation. Although operating endodontic rotary instruments in tooth canals was more appropriate for the clinical situation, the operation and immersion of endodontic rotary instruments were performed in a plastic tube to standardize the experimental comparative study. Moreover, the absence of friction between endodontic rotary instruments and dentin may lead to lower wear results, which may represent a limitation of this in vitro study. Further studies are recommended to be conducted using different concentrations and types of irrigants over different periods of immersion. Moreover, the changes in the chemistry of the Ni-Ti surface in response to exposure to irrigants may be useful to investigate using chemical elemental analysis.

Conclusions

The new TN and PTN Ni-Ti instruments showed the least surface roughness. Irrigations with 5.25% NaOCl for 15 min. affect the surface roughness of all tested Ni-Ti rotary endodontic instruments. CM and PTN Ni-Ti instruments exhibited the least surface roughness after irrigant exposure.

Abbreviations

Ni-Ti	Nickel-titanium
PTN	Protaper next
CM	Hyflex CM
EDM	Hyflex EDM
WOG	WaveOne gold
TN	Trunatomy
NaOCI	Sodium hypochlorite
Sa	Surface roughness average
AFM	Atomic Force Microscope
MREC	The Medical Research Ethical Committee
NRC	National Research Centre
3D	Three-dimension
2D	Two-dimension

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Authors' contributions

Tamer M. Hamdy, Amira G. Ismail and Manar Galal conceived the ideas; Tamer M. Hamdy, Amira G. Ismail and Manar Galal designed the study; Tamer M. Hamdy, Yasmine M. Alkabani, Amira G. Ismail, and Manar Galal collected and analyzed the data, Tamer M. Hamdy wrote the manuscript, Tamer M. Hamdy, Yasmine M. Alkabani, Amira G. Ismail, and Manar Galal read and approved the final manuscript.

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Data Availability

The data that support the findings of this study are available from the corresponding author upon reasonable request.

Declarations

Ethics approval and consent to participate

This in vitro study received ethical approval from the Medical Research Ethical Committee (MREC) of National Research Centre (NRC); Cairo, Egypt (Reference number: 24312012023). All methods were carried out in accordance with relevant guidelines and regulations. This study was carried out in accordance with the Declaration of Helsinki.

Consent for publication

Not applicable.

Competing interests

The authors declare that they have no competing interests.

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