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# Analysis of osseointegration of implants with macrogeometries with healing chambers: a randomized clinical trial

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## Abstract

**Background** To verify the influence of macrogeometry with healing chambers on the osseointegration of dental implants by analyzing implant stability quotient (ISQ) and evaluate the correlation between insertion torque and ISQ insertion with different macrogeometries.

**Methods** In total, 26 implants were installed in the posterior mandible of eight patients with sufficient bone height for the installation of implants measuring 3.5 mm in diameter and 9.0 mm in length. The implants were categorized according to two types of macrogeometry: a test group (GT) with 13 conical implants with healing chambers and a control group (GC) with 13 conical implants with conventional threads. To insert the implants, a bone drilling protocol was used up to a diameter of 3 mm with the last helical bur. The insertion torque of the implants was evaluated, followed by the measurement of ISQ at 0 (T-0), 7 (T-7), 14 (T-14), 21 (T-21), 28 (T-28), and 42 (T-42) days.

**Results** The mean insertion torque was 43 Ncm in both groups, without a significant difference. Moreover, no significant difference in the ISQ values was found between the groups at different time points ( $p > 0.05$ ), except at T-7 (GT =  $69.87 \pm 1.89$  and GC =  $66.48 \pm 4.49$ ;  $p = 0.01$ ). Although there was no significant difference, ISQ median values were higher in the GT group than GC group at 28 days (GT = 67.98 and GC = 63.46;  $p = 0.05$ ) and 42 days (GT = 66.12 and GC = 60.33;  $p = 0.09$ ). No correlation was found between the insertion torque and ISQ insertion ( $p > 0.05$ ).

**Conclusion** Furthermore, implants with a 3.5 mm diameter macrogeometry, with or without healing chambers, inserted with a drilling protocol up to 3 mm in diameter of the last helical bur, led to a similar secondary stability, with

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no difference in ISQ values. Although, implants with healing chamber demonstrates ascending values in the graph of ISQ, having a trend of faster osseointegration than implants without healing chambers. Both macrogeometries provide a similar primary stability to implants.

**Trial registration** This study was registered retrospectively in ReBec (Brazilian registry of clinical trials) under the number RBR-96n5x69, on the date of 19/06/2023.

**Keywords** Dental implants, Osseointegration, Healing chambers, Mandible

## Introduction

Osseointegration is currently defined as the contact established without the interposition of non-osseous tissue between the remodeled normal bone and an implant, implying sustained transfer and load distribution from the implant to and within the bone tissue [1]. In precursor implants, the time of osseointegration in the mandible was recommended to be 3 months, and in the maxilla, 6 months [2]. Over the years, there have been constant improvements in the geometry and surface of implants as an attempt to accelerate osseointegration [3, 4].

Previous studies have shown that less bone compression in the implant insertion bed results in less tissue trauma and, consequently, less intensity of the inflammatory process [5–7]. Over-drilling, when the diameter of the last drill used in the bed approaches the external diameter of the threads, can also contribute to the reduction of this inflammatory process by lower compression of the implant surface on the bone, resulting in lower insertion torque [6]. Thus, studies with healing chambers, different types of threads, and drilling techniques have been developed to evaluate secondary stability and analyze different degrees of bone compression for a better osseointegration in macrogeometries with less compressive behavior [8–11].

Although few studies have prioritized over-drilling protocols for lower bone compression and acceleration of secondary stability, others have shown rapid osseointegration with conventional drilling protocols in Straumann implants (Straumann – Basel, Switzerland) [12, 13]. This company advocates a drilling protocol for most of its implants, with the last helical bur approximately 0.6 mm smaller than the diameter of the implant to be inserted, such as the use of the last 3.5 mm bur to insert a regular 4.1 mm implant. This conventional drilling protocol provides osseointegration in approximately 4 to 6 weeks, with an insertion torque ranging from 30 to 60 Ncm for the Straumann (Straumann – Basel, Switzerland) system on Standard Plus, Bone Level, and Tissue Level implants [14, 15].

Surface treatments of implants with sandblasting and acid attack increase surface roughness and implant-bone contact, improve the quality of osseointegration, and reduce bone repair time, providing attraction and adhesion of osteoblasts [16]. Implants subjected to

sandblasting and acid attack have demonstrated a high survival rate (99%), promoting osseointegration within 6 weeks [13, 17, 18].

Macrogeometric, microgeometric, and surgical protocols for bone bed preparation and implant insertion interfere with osseointegration [17, 19–22]. The Due Cone implant (Implacil de Bortoli, – São Paulo, SP, Brazil) is a conical implant manufactured from commercially pure grade IV titanium, has a progressive trapezoidal thread design and surface treatment with the blasting of titanium oxide microparticles (approximately 100 µm) with subsequent etching with maleic acid [23]. Good results for implants with this macro design and surface treatment have been reported, in addition to the occurrence of osseointegration within 6 weeks of insertion [3, 18, 21]. Additionally, these implants have shown similar results to implants from other brands, such as Straumann and Nobel Biocare (Göteborg, Sweden), in animal studies, regarding the percentage of bone in contact with the implant (BIC%) after 6 weeks of healing [3, 23].

The presence of healing chambers on the surface of dental implants raises the hypothesis of acceleration of traditional implant osseointegration, aiming at shorter prosthetic rehabilitation on the implant [8, 11]. The Due Cone implant underwent modification in its macrogeometry with healing chambers to increase the implant and bone contact area, favoring the idea and concept of “less bone compression” during implant insertion. Animal studies carried out with this implant system, comparing conventional macrogeometry and macrogeometry with healing chambers, showed favorable bone accumulation in the healing chambers and reduction of implant insertion torque without loss of primary stability [8–10].

Osstell (Integration Diagnostics AB, Göteborg, Sweden) measures the stability of the implant during certain periods of bone repair after its insertion. It allows the assessment of the stability of implants by resonance frequency assessment (RFA), which is generated by a magnetic pulse transmitted by a portable instrument that excites the SmartPeg. Thus, the implant stability quotient (ISQ) was obtained on a scale of 1 to 100.21 This assessment is widely used to analyze the implant stability and is related to the lateral stability of the implant, which depends on the rigidity of the connection between the implant surface and bone [22, 24–27].

This study aimed to evaluate the osseointegration and primary stability of two implant macrogeometries inserted in the mandible using a conventional drilling protocol. The analysis focused on the ISQ in the initial phases of bone healing and examined insertion torque and insertion ISQ, as well as the correlation between these measures. We hypothesized that the healing chambers could accelerate the process of osseointegration under the evaluated conditions by increasing the ISQ in a 42-day time period.

## Materials and methods

### Study design

This randomized clinical trial analyzed the insertion of 26 implants in the posterior region of the mandible of eight patients by comparing the ISQ values of two different types of implant macrogeometry. The patient recruitment period for this study began on April 7, 2022 and ended on June 2, 2022. The surgery to insert the implants was carried out in July 2022 with a follow-up of 42 days after the implant insertion surgery. Patients were categorized according to the type of implant macrogeometry: a test group (GT; with healing chambers; Maestro, Implacil de Bortoli, São Paulo, SP, Brazil) and a control group (GC; with conventional threads; Due Cone, Implacil de Bortoli, São Paulo, SP, Brazil). This study was approved by the Ethics and Research Committee of Pontifícia Universidade Católica do Paraná (PUCPR - number 5.338.876) and was retrospectively registered in ReBec (brazilian registry of clinical trials) under the number RBR-96n5×69. Informed consent was obtained from all individual participants included in the study. This study was conducted in accordance with CONSORT reporting guidelines [28].

### Patient selection

Patients aged over 21 years that needed implants in the mandibular posterior region were selected. Patients assisted at the dental clinic of PUCPR were pre-selected based on the evaluation of panoramic radiographs. After pre-selection, patients who met the eligibility criteria were invited to a consultation with a clinical examination and referred to the radiology sector for cone-beam computed tomography and were included in the study. The sample was collected by convenience and after a sample power test was carried out to determine the significance of the sample.

The inclusion criteria were as follows:

- patients with partially edentulous posterior mandible requiring one implant in each half-arch or two implants in each half-arch;
- those with a minimum bone height of 11 mm and minimum bone thickness of 5 mm in the posterior

region of the bilateral mandible evaluated using cone beam computed tomography; and.

- those with sufficient prosthetic space for subsequent prosthetic rehabilitation.

The exclusion criteria were as follows:

- Patients who require some type of bone reconstruction or advanced surgery to allow implant installation;
- patients who did not agree to be part of the study;
- patients with uncontrolled diabetes, with glycated hemoglobin (HbA1c) above 7.5%; [29]
- smokers (> 10 cigarettes/day);
- those using oral or injectable bisphosphonates;
- immunodeficient patients.
- patients who underwent radiotherapy in the head and neck region for less than 5 years before the beginning of the research;
- patients with another systemic condition that contraindicated performing oral surgery or those who had conditions that could interfere with osseointegration.

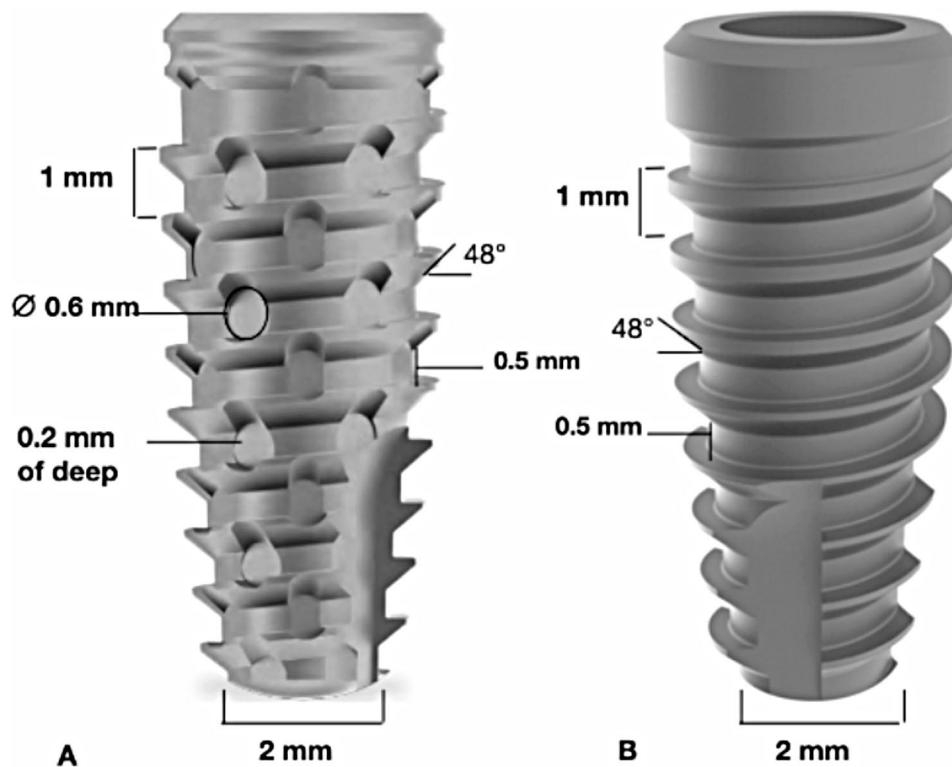
### Allocation randomization and blinding

Each patient underwent surgery to install implants with healing chambers (Maestro) and conventional threads (Due Cone). All implants used were conical with a conical internal connection of size 3.5×9 mm. Randomization of the sites of each implant was performed by drawing lots with a sealed opaque envelope for each site of the mandible, thus creating a test group (GT) of Maestro implants and a control group (GC) of Due Cone implants. The patient and examiner who performed the clinical evaluations were blinded; however, it was not possible to blind the dentist who performed the procedure. The treatment allocation is shown in Fig. 1 and the macrogeometry of the implants used is shown in Fig. 2.

### Intervention

Plans were made to perform the surgeries based on clinical evaluations and image analysis of cone-beam computed tomography scans. All biosafety procedures were adopted, and medications were prescribed before and after the surgery. One hour before the surgery, 2 g of cefadroxil was prescribed. To reduce pain and inflammation after the surgery, 100 mg of ketoprofen and 750 mg of paracetamol were prescribed for 3 days. Patients were instructed to use a mouthwash containing with 0.12% of chlorhexidine twice daily for 7 days.

Patients were anesthetized with 4% of articaine with 1:100.000 epinephrine (DFL, Rio de Janeiro, RJ, Brazil) using the inferior alveolar nerve block technique,



**Fig. 1** (A) Implant test group with healing chambers; (B) Control group implant without healing chambers

complemented with the local infiltrative technique. A linear incision was made using a 15c scalpel blade in the bone crest. The detachment of the flap was performed with a Molt detacher, and the demarcation of the perforation site was started with the spear drill mounted on a 20:1 contra-angle until the desired height. Irrigation was performed with saline solution, and perforations were performed with the corresponding 2.0 conical burs and the 3.0 conical bur. Implants were installed 1 mm below the bone crest with a contra-angle to a torque of 35 Ncm and were finished with a surgical torque meter (Implacil de Bortoli, São Paulo, SP, Brazil) to verify the insertion torque.

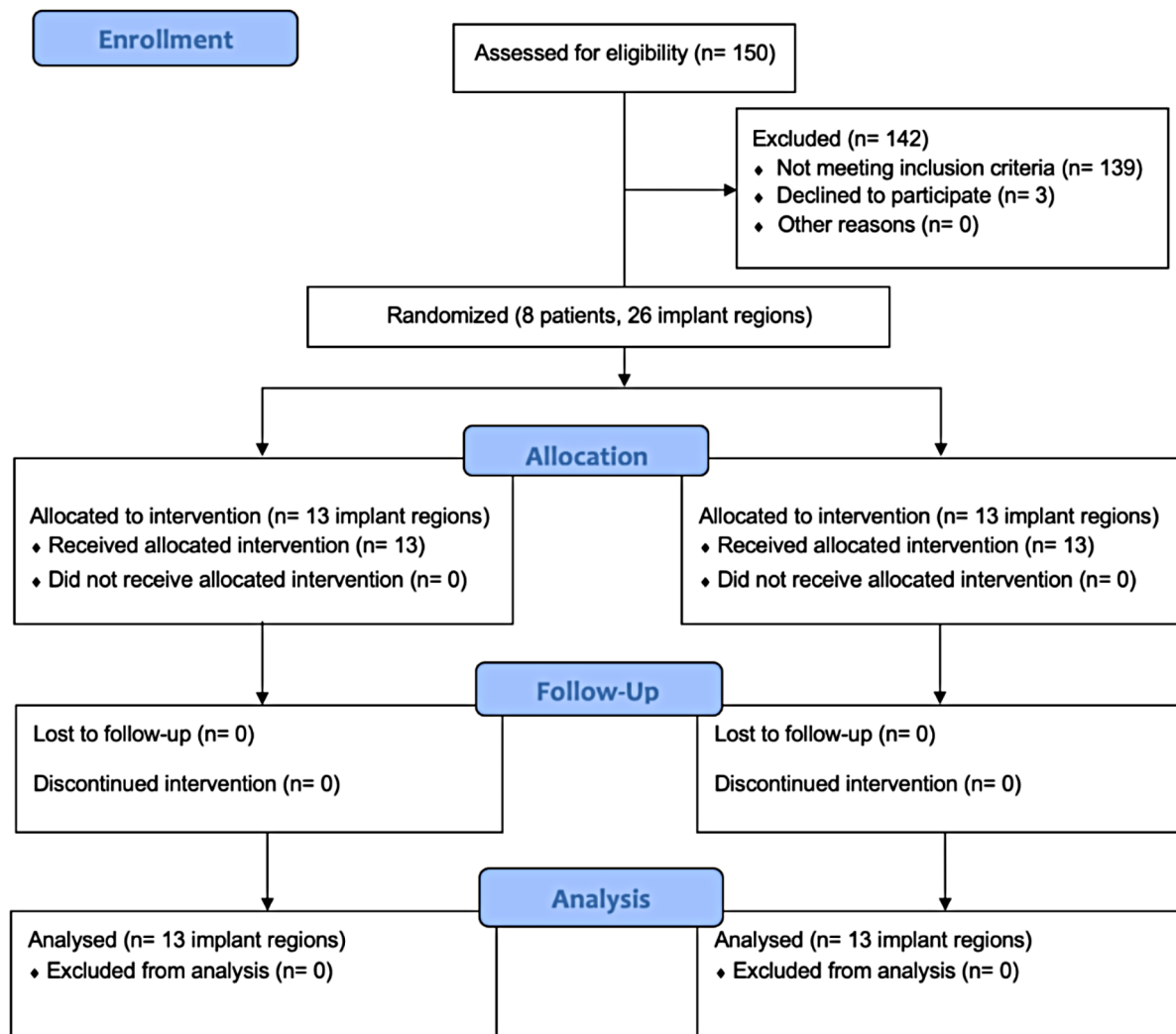
All implants were installed using the Bortoli Implacil kit. A conventional drilling with a drill up to 3.0 mm was used, unlike the manufacturer's recommendation, which recommends the last reamer of 3.5 mm, to test this drilling protocol on all implants of both groups. If the implant achieved a torque greater than 60 Ncm, it was removed, and a 3.5 mm drill of the drilling sequence was used so that the insertion torque was not high to prevent marginal bone loss at the sites. The insertion torque of each implant was checked, and a SmartPeg was installed directly on the implant to assess the primary stability by resonance frequency. Subsequently, a mini-abutment (Implacil de Bortoli, São Paulo, SP, Brazil) was installed with a torque of 20 Ncm with a prosthetic torque meter

and specific wrench. The surgical procedure was completed with a 5.0 nylon suture thread.

#### Assessment of primary and secondary stability

Primary stability was evaluated by the insertion torque values of each implant, and compared to their implant stability quotient (ISQ) values with the Ostell instrument (Integration Diagnostics AB, Göteborg, Sweden), both directly on the implant and on the mini-abutment installed. The ISQ assessment in the post-implant installation period was performed on the mini-abutment to facilitate this assessment and avoid overloading the healing implant [30]. At the time of implant installation, the ISQ assessment can be performed directly on the implant without damaging it [31].

The RFA test was performed at the time of implant installation directly on the implant, on the mini-abutment on the day of installation, and on the same mini-abutment after 7, 14, 21, 28, and 42 days. RFA produces an ISQ that ranges from 1 to 100; a higher ISQ value indicates a greater clinical rigidity. At each measurement visit, SmartPeg was installed on the mini-abutment with a torque of 10 Ncm, and the measurements were repeated. The ISQ was measured by the same independent examiner in four different positions (mesial, distal, lingual, and buccal) perpendicular to the SmartPeg (Fig. 3). The mean values were considered as the value of primary or secondary stability when measured on the day of implant



**Fig. 2** Patient selection and allocation diagram, according to CONSORT

installation or during follow-up, respectively. Measurements were performed independently, evaluating one implant at a time, the examiner blinded of the group, and SmartPegs were individualized for each implant.

In all follow-up consultations, clinical evaluations were performed to investigate the edema and signs of infection, and the patient was enquired about the presence of postoperative pain and discomfort.

#### Statistical analysis

Data were analyzed using a statistical program (SPSS 25.0, IBM Statistics, New York, NY, USA). The Shapiro–Wilk test showed a non-normal data distribution. The correlation between the insertion torque and ISQ at the time of implant placement was analyzed using Spearman’s non-parametric test. The non-parametric Mann–Whitney U test was used to assess the differences between the groups, and the Friedman test was used to assess the difference between the ISQ results in

the samples at different times. The sample power test was performed to determine the significance of the sample. Tests were performed at a significance level of 5%.

#### Results

In total, 26 implants were placed in the posterior region of the mandible in eight patients (women, 7; man, 1) aged between 38 and 69 years. All implant insertion sites were randomized, resulting in 13 implants in the GC group and 13 implants in the CT group evaluated.

In the analysis between groups at different evaluation times, there was a statistically significant difference at T-7, with higher ISQ values for the GT ( $p=0.01$ ; Table 1). Although there was no significant difference in the other times, ISQ median values were higher in the GT group than GC group at 28 days (GT=67.98 and GC=63.46;  $p=0.05$ ) and 42 days (GT=66.12 and GC=60.33;  $p=0.09$ ). Table 1 shows the mean values, standard deviation, median, and interquartile range of insertion torque,



**Fig. 3** Evaluation of the implant stability quotient with Osstell

ISQ on the implant at T-0, and ISQ on mini-abutment at all times points.

No statistically significant correlation was found between the insertion torque and ISQ at the time of installation ( $p > 0.05$ ) (Table 2).

In the Friedman test, there was a significant difference in terms of the ISQ results at different time points, both for the total sample ( $p = 0.004$ ) and the samples of the GT ( $p = 0.035$ ) and GC ( $p = 0.043$ ), showing higher values over time.

A sample power of 77.2% was obtained for ISQ values at T-7 ( $p = 0.01$ ), confirming the statistical power of this sample for this time point.

Figure 4 presents a graph with Q1, Q2 (median), Q3, and minimum and maximum ISQ values on the mini-abutment at different time points.

### Discussion

Implant characteristics have been improved to achieve ideal secondary stability in a short period of time [32, 33]. Already well documented in the literature and widely known by clinicians, Straumann implants have rapid osseointegration, and Both GT implants (Maestro Implants) with trapezoidal threads and Straumann implants with conventional threads present with low insertion torque or locking [10]. The same is evaluated by

**Table 1** Values for insertion torque and ISQ at the evaluated times

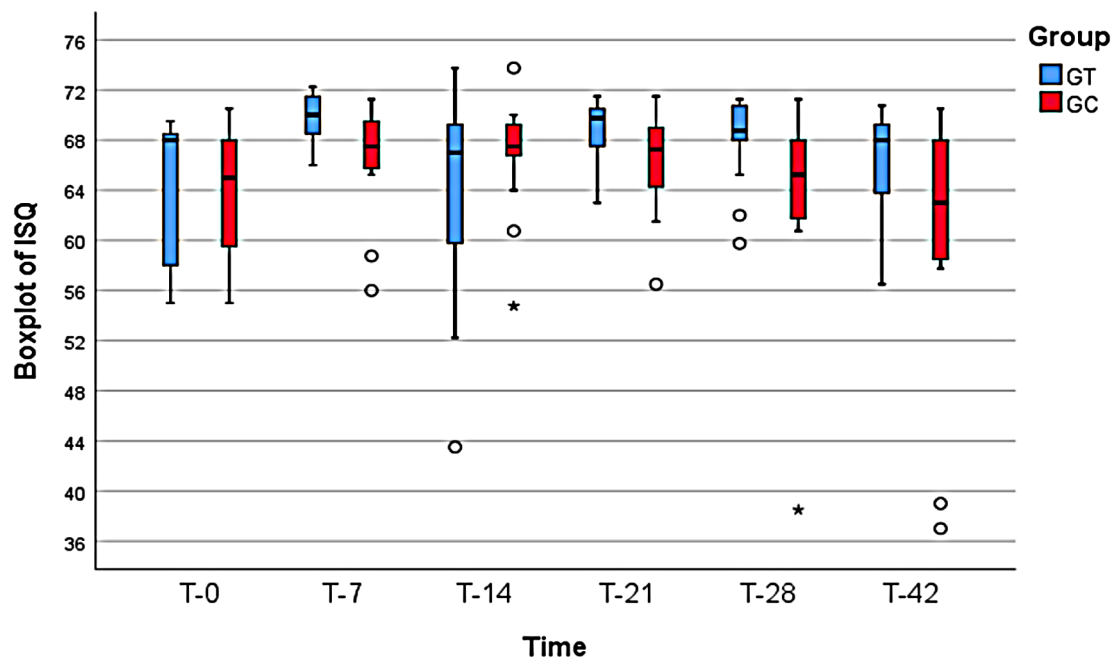
Variable	Group	n	Mean	Standard deviation	Median	AIQ	p value Mann-Whitney U test
Insertion torque T-0	GT	13	42.92	10.78	40.00	20.50	0.61
	GC	13	43.46	10.68	45.00	7.50	
Implant ISQ T-0	GT	13	58.37	8.00	56.75	13.00	0.89
	GC	13	57.75	15.74	61.25	23.00	
Mini-abutment ISQ T-0	GT	13	64.85	5.47	68.00	10.75	0.43
	GC	13	63.60	5.11	65.00	8.88	
Mini-abutment ISQr T-7	GT	13	69.87	1.89	70.00	3.50	0.01
	GC	13	66.48	4.49	67.50	4.50	
Mini-abutment ISQ T-14	GT	13	64.27	8.58	67.00	10.38	0.57
	GC	13	66.83	4.77	67.50	4.13	
Mini-abutment ISQr T-21	GT	13	68.58	2.78	69.75	4.50	0.07
	GC	13	66.31	4.02	67.25	5.25	
Mini-abutment ISQ T-28	GT	13	67.98	3.57	68.75	4.13	0.05
	GC	13	63.46	8.22	65.25	7.25	
Mini-abutment ISQ T-42	GT	13	66.12	4.38	68.00	7.13	0.09
	GC	13	60.33	10.62	63.00	9.88	

AIQ: interquartile range = Q3 - Q1. TG= Test Group; GC= Control Group; ISQ= Implant Stability Quotient. Mann-Whitney U test for difference in ISQ between groups at different evaluation times performed with 5% significance ( $p > 0.05$ )

**Table 2** Correlation of the sample between insertion torque and ISQ at the time of installation

Variable	Correlation coefficient	Insertion torque T- 0	Mini-abutment ISQ T- 0
Insertion torque T- 0	Correlation Coefficient	1	0.052
	p value		0.79
	N	26	26
Mini-abutment ISQ T- 0	Correlation Coefficient	0.05	1
	p value	0.79	
	N	26	26

T-0: evaluation performed during the installation of implants



**Fig. 4** Boxplot graph of ISQ values between the evaluated groups, at different times

a torquemeter: the low torque of the test implants can be conferred by the healing chambers, while the low torque of the Straumann control implants can be verified by the type and shape of the threads. Despite the mechanical torque being low in both types of implants, the secondary stability performance is comparable, with ISQ results close to 70 at 28 and 42 days, indicating a good stability value closer to 70. In the present study, the values of ISQ in the GT at 28 and 42 days were 68; These values were close to the ISQ values of 70 presented in the group of implants with the same characteristics installed in the rabbit tibiae [10].

The primary stability of the implant must be obtained to achieve the desired bone healing, with new bone formation around the implant and its maturation without the formation of connective tissue [34]. For this, the implant needs to remain static in the bone, respecting its primary stability [35]. However, the high insertion torque can impair the optimal healing of the implant in the bone tissue by osseointegration, and the development of implants with smoother threads and smaller lengths and depths of chambers between the threads is increasingly widespread [36]. Thus, a final consensus advocates an ideal insertion torque value between 30 and 50 Ncm, and torques above this value may impair the osseointegration [37]. In our study, the mean insertion torque was approximately 40–45 Ncm, which is within the recommended value. Previous studies have indicated the excellent performance of the Straumann SLA implant, both in its reduced osseointegration time and the amount of newly formed bone in close contact with the implant [17, 18,

38]. In addition to the surface treatment, this characteristic may also be due to the low value of insertion torque due to the softer and less compressive threads, in addition to the low length of chambers between the implant threads. Implants with healing chambers (Maestro implants) showed higher ISQ and BIC% (bone-implant contact) values than those with Straumann implants 28 days after their insertion in rabbit tibiae [10]. These values in animals show a similarity between the Straumann and Implanil Maestro implants with healing chambers.

In this study, the healing chambers on the surface of the implant in the GT provided an increase in the contact area between the implant and the bone while reducing the insertion torque and bone necrosis around the implant [8, 9]. This characteristic tends to increase the BIC area, reducing the time of secondary stability of the implant and consequently reducing the healing time of the implant in the bone, allowing an opening of the implant to perform the definitive prosthesis in less time [8, 9]. In the present study, it was not possible to assess the BIC% value because it was a human study; Although there is no statistically significant difference between the ISQ of both groups tested in our study, the mean and median values of ISQ in GT for 28 and 42 days are higher, which may indicate an acceleration trend of osseointegration and a possibility of earlier prosthetic loading in implants with healing chambers.

Some in vitro studies show that the primary stability of implants with and without healing chambers is similar because the insertion ISQ of these implants is similar, although the insertion torque is lower in implants with

healing chambers [39–41]. Animal studies show higher ISQ and BIC% values in the group of implants with healing chambers than in implants without chambers, after a period of 4 weeks [8, 9, 11]. Our study showed no difference in insertion ISQ between the groups, corroborating the literature confirming good primary stability of the tested implants, in addition to also showing good secondary stability.

In the present study, a conventional drilling protocol was used with the last helical drill cutter 0.5 mm smaller than the inserted implant diameter for both groups, but when the implant was inserted with a higher torque, above 60 Ncm, the implant was removed, and an optional 3.5 mm diameter drill was used so that the insertion torque was not high. The values of both insertion torque and insertion ISQ were very close between the groups, which may be due to the standardization that we obtained in our study. To improve the primary stability, especially in more medullary bone, such as type IV bone [42], under-drilling performed with drills with a 0.6 to 1.5 mm difference in implant diameter can increase implant locking, especially in those with a low insertion torque due to the macrogeometry and presence of a more medullary bone [7, 40, 43–45]. In implants with macrogeometry that confers a high locking, sub-drilling in more cortical bone (types I and II) [42] is not recommended because the insertion torque becomes higher with a greater probability of bone necrosis in the bed and results in greater marginal bone loss [7, 46]. The greater compression may occur due to the thread geometry of the implant, having a greater compression with more aggressive threads for greater locking [47]. When there is an excessive compression of the implant in the bone due to the high insertion torque of the implant, forces are transmitted to the adjacent bone, which may cause irreversible damage and reach a maximum threshold with plastic deformation, microcracks, and even necrosis [48]. Greater damage tends to occur mainly in the cortical bone, which does not have a good blood supply and is more easily reabsorbed by necrosis [49].

The manufacturer of the implants used in this research recommended the use of drills up to 3.5 mm for the insertion of implants of 3.5 mm in diameter (types I and II) in the mandible region. This protocol favors decompression of the implant walls in the bone bed, thereby reducing the implant insertion torque [8–11, 39, 40]. This study did not follow the manufacturer's recommendation because we used a conventional drilling protocol in which the last reamer is 0.5 mm smaller in diameter than the diameter of the installed implant. This protocol is widely recommended by several implant manufacturers, including Straumann implants, which mostly have a drilling protocol with the last helical reamer in a 3.5 mm diameter for regular implants of 4.1 mm in diameter,

providing rapid osseointegration [14, 15, 50]. The Straumann Tapered Effect and Bone Level implants are self-tapping implants, different from the Straumann Standard Plus implant. These self-threading implants, with the same conventional drilling protocol (last drill 3.5 mm for implants of 4.1 mm in diameter), have a higher insertion torque than Standard Plus implants; however, they have similar osseointegration from 4 to 6 weeks, resulting in an ISQ above 70 in this period [50]. Herein, we aimed to adopt a conventional drilling protocol to test whether the macrogeometry influences the secondary stability in these conditions, similar to most systems because the risk of loss of insertion torque in implants installed with over-drilling (last drill similar to the diameter of the implant) can be considerable. Thus, in our study, we obtained an insertion torque pattern of 43 Ncm in both groups, with no difference between the values of both insertion ISQ and ISQ in subsequent evaluations, which may have been influenced by the established drilling protocol.

Surface treatment also influences the primary and secondary stability of the implant [16, 20, 21, 51]. The implants in the groups GT and GC underwent surface treatment using blasting titanium oxide microparticles ( $\cong 100 \mu\text{m}$ ), and were washed ultrasonically with alkaline solution and distilled water and submitted to the application of maleic acid, resulting in roughness of  $R_a=0.56 \pm 0.10 \mu\text{m}$ . In vitro studies carried out with the same implant tested in our study with healing chambers revealed higher values for implant removal torque and a higher bone fraction occupancy rate (BAFO%) in implants with healing chambers with treated surfaces than in implants with a machined surface [9]. Traditional implants with surface treatment provide better performance and a shorter time to reach secondary stability, with greater bone production on their surface, when compared to implants without surface treatment [52–54]. The implant used in this study has a roughness of  $R_a=0.56 \pm 0.10 \mu\text{m}$ ; however, one study found a greater differentiation and recruitment of osteoblasts on surfaces with medium roughness, around 1–2  $\mu\text{m}$  of roughness [55]. Therefore, improving the surface treatment and presence of healing chambers is recommended for better secondary stability.

In the present study, the ISQ values in the GT group were  $<70$ , despite being close to this value. In ideal values for the load on the implant, the Osstell manufacturer recommends ISQ values of  $\geq 70$  [56]. Therefore, based on the results of the present study, it may be imprudent to indicate load application with the installation of a definitive prosthesis in the period of 42 days for implants tested in the mandible with a conventional drilling protocol. However, the implants in the GT tended to have a shorter osseointegration time than the implants in the GC group,



probably not requiring an osseointegration time of 90 days in the mandible.

As for the limitations, despite being a prospective and randomized clinical study with a higher level of scientific evidence than a cohort study, since the researcher controls the actions and clinical follow-up, it was difficult to obtain a larger sample of patients due to recruitment and selection criteria eligibility, and specific time to follow the entire sample [57]. A sample with less than 30 participants is able to estimate data characterized by a population when specific statistical tests are applied according to their distinction of normality; however, in a larger sample, the statistical differences become more evident as the discrepancies of some values that do not follow the general average do not have much influence [58, 59]. In addition, we tested implants with a different drilling protocol than that recommended by the manufacturer. This may have influenced the results obtained, as studies of animals with the drilling protocol recommended by the manufacturer showed a significant difference between ISQ after 28 days, between implants with and without healing chambers [8–10]. Regarding the demographics of the patient sample, we believe that there was no interference in the results, since we kept the sample very similar with the eligibility criteria, since all patients were healthy, without any different health conditions, did not take continuous medication and did not have any type of addiction. Regarding clinical characteristics, we matched the position of the implant in the posterior region of the mandible, all having antagonists in the maxilla. With these similar characteristics, we believe that these factors did not interfere in the result. Although most studies test the ISQ for up to 45 days, it would be prudent to have future studies that test this value for a longer period to evaluate the pattern of bone healing over time to ensure that this pattern is ascending and that it does not decrease in values as it could affect the time of prosthetic implementation and prosthetic functionality. Therefore, it is recommended to develop future randomized clinical trials with implants that have decompression chambers compared to the same type of implant without them, inserted with the drilling protocol recommended by the manufacturer, to assess whether this device can influence the acceleration and quality of osseointegration, seeking to define an ideal prosthetic loading time protocol for these implants inserted in the mandible and maxilla.

## Conclusion

Regarding secondary stability, no difference was observed between the implants tested with the two macrogeometries, inserted with a conventional drilling protocol, and evaluated for a period of 42 days. Therefore, the healing chambers did not influence the implant stability quotient

(ISQ) values, providing secondary stability similar to that of the group without healing chambers.

Implants with and without healing chambers, inserted using a conventional drilling protocol, did not show different values for insertion torque and insertion ISQ, and there was no correlation between these values.

Although there is no significant difference between the groups, healing chambers may tend to accelerate osseointegration of implants, being feasible to apply prosthetic loading earlier than implants without healing chambers. Though, more clinical studies should be carried out to verify the secondary stability of these implants inserted both with the drilling protocol recommended by the manufacturer and with the conventional drilling protocol.

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## Author contributions

Conceptualization, P.T.R.S., R.M. and G.F.F.G.; Statistical analysis, S.A.I.; Formal analysis, P.T.R.S.; Methodology, P.T.R.S., R.M., F.A.O.S.S., N.F.M., B.E.S.A.F.M.; Project administration, L.R.A.-A. and E.A.R.R.; Resources, R.M.; Supervision, L.R.A.-A. and E.A.R.R.; Writing—original draft, P.T.R.S.; Writing—review & editing, R.M., L.R.A.-A., E.M.S. and E.A.R.R.

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## Data availability

All data generated or analysed during this study are included in this published article.

## Declarations

### Ethics approval and consent to participate

This study was approved by the Ethics and Research Committee of Pontifícia Universidade Católica do Paraná (PUCPR - number 5.338.876) and was registered in ReBec (Brazilian registry of clinical trials) under the number RBR-96n5x69. Written informed consent was obtained from all individual participants included in the study.

### Consent for publication

Not applicable.

### Competing interests

The authors declare no competing interests.

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